

Comparison of Different Dosimetric Indices for Volumetric Arc Modulated Treatment Planning Using 2 Different Treatment Planning Systems: A Feasibility Study for Total Body Irradiation

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Abstract

Objective: To compare two different treatment planning systems (TPSs) for plan quality and to check the feasibility of VMAT TBI on the Elekta linear accelerator 'Versa HD'. **Methods:** Ten clinical VMAT TBI plans were replanned in Monaco TPS version 5 for retrospective dosimetric analysis and to check the feasibility of treatment delivery in Elekta Versa HD. A dose of 12 Gy in 6 fractions was prescribed to cover 95% PTV. The OARs were the lungs, kidneys, heart, liver, and brain. Dosimetric optimization and calculation were performed in Monaco TPS with a statistical uncertainty of 1%, 2 mm grid. The chosen criterion for plan evaluation and comparison was based on plan quality, dosimetric indices like conformity and homogeneity index, and OAR doses. The comparison of time for optimization, monitor units, and beam on time was also analyzed. Pre-treatment verification using Octavious phantom and gamma analysis using Low's method with a dose difference of 3% and distance to agreement 3mm criteria was done. The dosimetry of 2 VMAT TBI plans were compared using Wilcoxon signed rank test. **Result:** The calculated average maximum and mean doses of the PTV were 14.3321Gy and 12.235Gy for Eclipse; and 14.428Gy and 12.198Gy for the Monaco system, respectively. The planning time in Monaco was approx. 4.5–6hrs compared to 14–18hrs for Eclipse TPS. Statistically significant difference was observed between the results of 2 TPSs in terms of monitor units, mean doses to lungs, kidneys, heart, and liver and planning time ($P < 0.05$). However, calculated p values for HI, CI, and brain for both VMAT TBI plans were not statistically different. **Conclusion:** The study showed the feasibility of VMAT TBI for VERSA HD as it offers faster, better optimization in a single target compared to the Eclipse.

Keywords: VMAT- TBI- OAR- AAA- MC- MU

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Introduction

Total body irradiation (TBI) is a radiation technique that is frequently used as a conditioning regimen for allogeneic hematopoietic stem cell transplantation (HSCT) or bone marrow transplantation (BMT) with chemotherapy [1]. The first study which showed that "stem cells" could recapitulate the blood system was reported by Till and McCulloch in the 1960s [2]. TBI used in conjunction with chemotherapeutic agents has proven to be useful for eradicating malignant cells from the blood formation sites. It also performs an immune-suppressive role by preventing

rejection of donor hematopoietic cells, aiding successfully BMT, and leading to superior treatment outcomes for HSCT [3-4]. TBI was developed to irradiate the whole body uniformly with a prescribed dose while minimizing radiation induced complications mainly to the lungs and kidneys. A dose uniformity of $\pm 10\%$ was accepted in TBI [1, 5]. Initially, TBI was given with parallel opposed field or extended source skin distances (SSD) or other conventional methods which had their limitation like fabrication, a time-consuming process in addition to acute

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and late toxicities as sparing of OARs was difficult [6]. Also, setup errors of a few millimeters in the longitudinal direction at the junction volume can produce dose inhomogeneity [7]. The feathering technique can help to reduce dose inhomogeneity in which the longitudinal location of the junction is varied across treatment fractions [8]. But this process was cumbersome, time-consuming, and required multiple setups. To overcome these difficulties of traditional treatment techniques, many new systems are available in which overlapping fields/arcs can be used at different iso-centers. Gradient dose-based optimization (GDO) technique use gradually decreasing/increasing junction volumes and base/bias dose option through inverse planning to deliver homogeneous dose with better sparing of OARs. Tomotherapy based VMAT TBI allows better OAR's sparing along with good homogeneous dose coverage of the target [9]. However, the attempt to deliver a clinically acceptable plan to the whole body only results in complicated planning which is mainly dependent upon the particular available treatment planning system (TPS) and dose delivery methods. Eclipse uses the PRO 3 optimization and AAA for dose calculation algorithm while Monaco is a Monte Carlo (MC) based algorithm, which uses 3 beam model components: transmission probability filters (TPFs), virtual source model (VSM), and X-ray voxel MC engine to achieve dose calculation accuracy. Monaco performs 2 stage optimizations: fast pencil beam for ideal fluence generation/distribution and the segmentation process includes segment shape, and segment weight for generating the best possible clinically deliverable VMAT TBI plans.

The aim of this retrospective study is to compare dosimetric quality and competency/efficacy of VMAT TBI plans generated on 2 different TPSs, 2 different delivery modalities using the same CT data sets in head-first supine position and to check for the feasibility of VMAT TBI on newly installed Versa HD linear accelerator in our institution.

Materials and Methods

1.1. Patient selection, contouring and dose prescription

Upper and lower body treatment planning computed topographic images with 5mm slice thickness of 10 selected patients were transferred to the Monaco TPS through Digital Imaging and Communication in Medicine (DICOM) with all delineated structure sets. All selected patients had already completed treatment on the Varian trilogly and pre-treatment QA was performed using the Artemis-Rapid Arc/VMAT QA Module of EPIQA [10]. To perform a meaningful evaluation and comparison, delineated PTV was given a 5mm inner margin after subtracting OARs. The included OARs for both the TPSs planning were brain, bilateral lungs, heart, liver, and kidneys. A single PTV optimization was performed in the Eclipse TPS. PTV was divided into three-four sub-PTVs as per the length of treatment to generate a clinically deliverable plan [11]. The bilateral lungs used for optimization were given a 2mm inner margin due to their proximity to the PTV and to deliver adequate

dose to marrow in the ribs. This may reduce conflicts to the optimizer attempting 2 different optimization parameters in adjacent contours. The prescribed dose to target volume was 12Gy/6#, 2# daily six hours apart. The objective was to cover 95% of the target with 90% of the prescribed dose. The PTV and other included OARs for each selected patient are shown in Table 1. The mean dose constraints for OARs were ≤ 10 Gy.

1.2. Planning Process and plan objectives

The Eclipse TPS-generated plans were used to deliver treatment in a Varian Trilogly linear accelerator. CT data sets from the Eclipse TPS through DICOM were exported to Elekta Monaco TPS version 5.11.03 and these were used to generate VMAT TBI plans for dosimetric verification on the VERSA HD unit. Eclipse uses Progressive Resolution Optimizer 3 (PRO3) for optimization and Anisotropic Analytical Algorithm (AAA) to calculate dose distribution from external photons. Both TPSs had different optimization and dose calculation algorithms. The Eclipse system accounts for tissue heterogeneity anisotropically in the entire three-dimension of interaction site and increases the accuracy of scattered dose calculation. The AAA has 2 components: a configuration algorithm and an actual dose calculation algorithm. But Monaco offers constrained optimization, which means the optimizer varies the plan to optimize the dose corresponding to user set objectives (i.e., dose to the target volume) while meeting OAR's hard constraints specified by the planner. Thus, the same planning parameters were chosen by fixing the same number and location of iso-centers, same field arrangement/overlapping junctions, longitudinal shifts, and same dose constraints. The same parameters used in both the plans in the study provided a meaningful and best possible dosimetric comparison. The dose delivery methods were also same in both the TPSs with static couch, moving gantry except collimation to the collimator head in Monaco.

1.2.1 Eclipse Planning

Treatment plan for the VMAT TBI was done using the Eclipse TPS version 11.0.31 from Varian to deliver on Varian Trilogly equipped with Millennium 60 pair multileaf collimators (MLCs). The outer 20 pairs MLCs have a 1 cm projection at the iso-center and the inner 40 pairs are projected 0.5 cm at the iso-center. The whole PTV was optimized with 2 pairs of arcs each at 4 different iso-centers. Multiple plans for the eclipse were made to achieve a deliverable plan. Different arcs were arranged to have an overlap region of 3 cm on the superior/inferior beam edges and one open field arc at the chest and abdomen iso-center to get a uniform dose distribution. The optimization and dose calculation time for a single PTV was approximately 6-8 hrs. The system also has a maximum limit of 10 arcs in one plan. Initially, for treatment delivery on eclipse PTV was divided into 4 different sub-PTVs to optimize for each PTV individually, in less time, and it also helped to avoid the maximum limit of arcs. Two arcs per iso-center clockwise (CW) and counter-clockwise (CCW) with one additional arc

at each iso-center with collimator rotation of 90° were used. The base dose tool was used to optimize different PTVs and smoothen doses at different arc junctions. After comparing the plan with four-different target plans, a good homogeneous deliverable plan was generated. The plan sum was the total plan consisting of arcs for different PTVs.

Monaco Planning TPS version 5.11.03 was used to create VMAT TBI plans for 10 selected patients. Monaco TPS employs the Monte Carlo (MC) algorithm, which is considered the most accurate algorithm available. The single PTV optimization was performed in 2 stages. The first stage used a fast Pencil Beam algorithm (PBC) to generate an ideal fluence distribution and the second stage optimized the shape and weight of the segment, so that a clinically deliverable plan could be generated.

2.2 VMAT TBI plan analysis, comparison, and verification

The clinically deliverable plans generated on both Eclipse and Monaco was normalized to deliver a 90% uniform dose to 95% of the target volume by subtracting the brain, the lungs, and bilateral kidneys. The field arrangement and overlapping region are shown in Figure 1 (a-c). VMAT TBI plans made on Monaco were analyzed and compared with plans generated on Eclipse. PTV mean and maximum doses, doses delivered to 95% of target, body maximum dose, and OAR mean doses were compared. Homogeneity index (HI) was calculated using D2% and D98% dose and D50% dose-volume histogram parameters and conformity index was calculated as per ICRU 83 definition [12]. The used formalism is:

$$HI = \frac{D_{2\%} - D_{98\%}}{D_{50\%}}$$

An HI of zero indicates that the absorbed-dose distribution is almost homogeneous. Analysis of total

MU's, planning, and dose delivery time was also done. Verification plans were created for both TPSs in already acquired PTW Octavius phantom large image data sets (50cm) and verified in synchronized rotational gantry angles using an inclinometer. The 2 measurements were taken for the phantom in face-in and face-out positions and composed together to find uniformity of doses at the different arc junctions and within arc fields. The gamma evaluations for quality assurance (QA) were done using Low's method for a dose difference between 3% and a distance agreement of 3 mm.

Results

Both TPS plans were compared for PTV coverage, OAR sparing, optimization and dose calculation time, MU's to be delivered, and beam on time. The dose coverage in different planes for both TPS plans is shown in Figure 2. The axial, coronal, and sagittal planes represent homogeneous dose distribution, proper dose sculpting, and OARs sparing in both TPSs.

1.1 PTV analysis

The Monaco TPS VMAT TBI plans resulted in good dose coverage of PTV than Eclipse plans. The average maximum and mean doses of planning target volume were 14.3827Gy±0.389Gy and 12.235Gy for the Eclipse; and 14.535Gy±0.164Gy and 12.198Gy for the Monaco system, respectively. HI for the PTV was comparable in both TPSs (Table 2). The CI was better in Monaco (p < 0.05). The comparative DVH for PTV for the two TPS plans is shown in Figure 3a. The variation of HI and CI for both TPSs was also plotted and is shown in Figures 4 (a and b).

1.2 OAR doses

The comparison of average mean doses received



Figure 1. (a and b). Beam Isocenters in Coronal and Sagittal Plane. 1(c) Displaying Isocenter and Overlapping Region.

Table1 Contoured Target Volume and OARs

Target Volume	Prescription Dose
PTV (up to mid-thigh)	12Gy/6#: 2Gy/# daily 2# 6 hourly apart
Lungs, Kidneys, Heart, Liver, & Brain	< 10Gy

PTV, planning target volume after subtracting both lungs and kidneys, liver, heart, and brain; B/L: bilateral

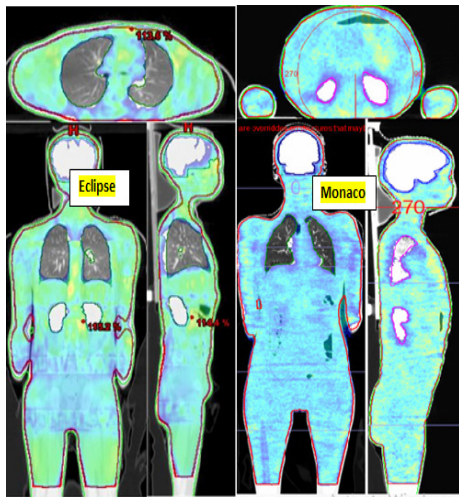


Figure 2. Dose Distribution in Axial, Coronal, and Sagittal Planes for Eclipse and Monaco

by the lungs, kidneys, liver, heart, and brain are shown in Table 3; a comparative DVH for OARs is shown in Figure 3b. The mean dose in the brain was comparable in the 2 TPS plans. The mean doses for lungs, kidneys, liver, and heart were higher for the Eclipse than Monaco, which was statistically significant ($p < 0.05$) and shown in Figure 5.

1.3 Monitor units, planning time and time for delivery

The total MUs for all arcs to be delivered were 2082.3 ± 473.9 , and 6681.4 ± 1210.2 , respectively for the Eclipse and the Monaco TPS (Table 2 and 4). For each iso-center, MUs were 694.13 ± 157.97 and 22273 ± 403.4 for the Eclipse and the Monaco plans, respectively. The Monaco plans MUs were approx. 3.2 times more than the Eclipse

TPS plans (Table 2). The average time to deliver a VMAT TBI plan in Versa HD was approximately 14–18 min but Varian trilogy took around 18-22 minutes.

Plan Verification

The plan verification was performed using Octavius phantom. The average gamma passing rate was 97.2% for the Eclipse and 97.6% for Monaco. Figure 6 shows a screenshot of the composed plan in the abdomen region. On 3D volume analysis, an average gamma was 98.1% and 97.8% for the Eclipse and Monaco, respectively. Figure 6 is displaying the average gamma passing point for the 3%, 3mm criterion.

Discussion

Total body irradiation is a useful conditioning regimen for patients undergoing BMT for hematological malignancies. In this study, we compared 2 different TPSs for plan quality and competency of VMAT TBI on the Elekta linear accelerator ‘Versa HD’. The average maximum dose in Monaco was 15.23cGy more than the Eclipse and the observed difference in average mean doses was 3.70 cGy which was not significantly different. The mean lung and kidney, liver, and heart doses were significantly higher for the Eclipse than Monaco but brain doses were similar. In this study, OAR doses were more than the mean lung dose threshold reported by Volpe et. al 9.8Gy versus 9.4Gy [8]. Our objective was to restrict the mean doses of the OARs to ≤ 10 Gy. From the HI and CI obtained in the current study, we can conclude that both the TPSs had the potential to create clinically deliverable plans with a good sparing of OARs. Our results was similar to those reported by Lu W., Adrian N., and Aleks [11, 13-15]. Planning and dose calculation time was

Table 2. Dosimetric Indices Comparison for the Two TPSs

PTV	Eclipse TPS	Monaco TPS	P
HI	0.22±0.03	0.18±0.03	0.051
CI95%	0.91± 0.02	0.91± 0.02	0.03
MU	2082.3±473.9	6681.4±1210.2	0.00000006

HI, homogeneity index; CI conformity index; MU, monitor unit; †Wilcoxin test P-value<0.05

Table 3. Mean OAR Doses in Gy for the two TPSs:

OARs (Avg_mean)	Monaco TPS (Avg_mean±SD)	Eclipse TPS (Avg_mean±SD)	P
Brain	10.105±0.4273	10.113±0.0474	0.954
Lungs	9.9724±0.3498	10.230±0.0634	0.049
Kidneys	9.9214±0.2672	10.252±0.1167	0.01
Liver	9.9883±0.062	10.1573±0.1206	0.00745
Heart	9.9403±0.1246	10.0775±0.1163	0.00436

†Wilcoxin test P-value<0.05

Table 4. MU’s for both TPSs

Pt. no.	1	2	3	4	5	6	7	8	9	10	Mean ± SD
MU_E	1814	2095	1872	2176	1879	2014	1567	1851	3309	2246	2082.3±473.9
MU_M	6530	7250	4942	5813	6384	7869	5178	6743	8929	7174	6681.2±1210.3

MU_E, monitor unit in Eclipse; MU_M, monitor unit in Monaco

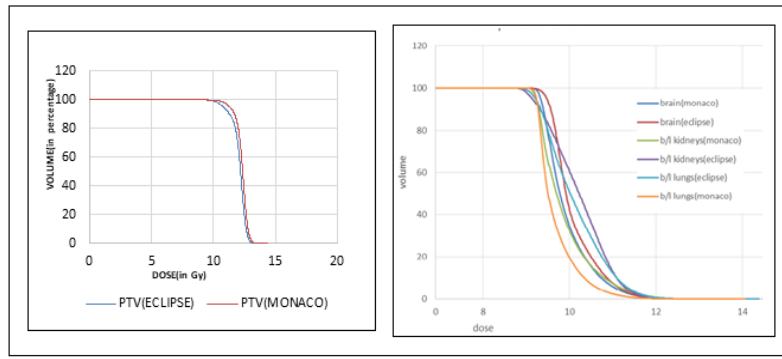


Figure 3. a) DVH for PTV in two TPSs; b) DVH for OARs in two TPSs

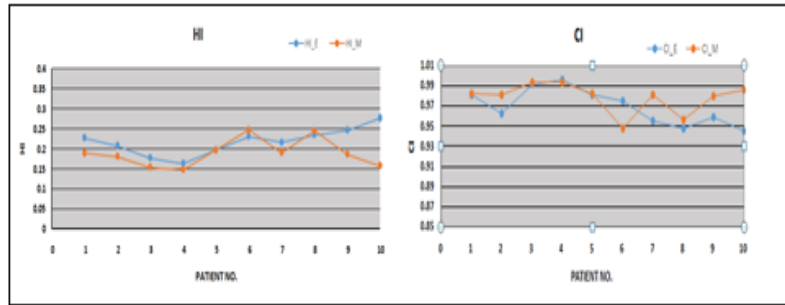


Figure 4. HI & CI Variation, E & M Represents Eclipse & Monaco, Respectively.

three times less for Monaco as compared to Eclipse. But a significant beam on time difference (2-4 minutes) was observed because MU's delivered were three times more in Monaco (Table 4 and 5). The more number of MUs is the result of algorithm difference of TPSs. The benefits of TBI are well published and documented [16]. In the presented study both TPSs produced comparable dose distribution in term of HI and CI.

A single PTV optimization in the Monaco TPS offers benefits for the planner rather than optimizing sub-PTVs in the Eclipse TPS for clinically acceptable plan generation. Although Eclipse TPS offers single PTV optimization it takes a longer time to complete optimization. Sometimes overlapping OARs in sub-PTVs create a conflict in achieving dose constraint. In a study, Springer et al. showed satisfactory dose distribution in the whole-body target for linac-based VMAT TBI in 7 patients using 9-15

iso-centers [17]. This large field planning of VMAT TBI is very complex due to multi-isocentric overlapping arcs. So necessary quality assurance tests are needed using an appropriate/ available phantom. In our study, we used 3-4 iso-centers with a 3cm overlap region. The dose distribution in the critical junction at the thigh region was controlled using base/bias dose properties in both the TPSs. The delivered doses were monitored to ensure that they were quite close to the prescribed dose, and this helped in dose adjustment of the fractional dose if needed.

In our study, we used an ionization chamber, gaf-chromic film, and diode to monitor the delivered dose. In a study, Springer et al. used MOSFET for measurements, and reported results were within 5% accuracy [17]. In another study, Ganapathy K et. al used the TLD-100 LiF and found that the dose homogeneity was within + 10% [18]. Various phantoms and detectors are available for dosimetric verification and any of them can be used for verification. Hui et. al. performed plan verification in their study using a cylindrical phantom [19]. Zhuang et. al. used a solid water phantom of 30 cm x 30cm x 12cm with gaf-chromic film and a 0.6cc farmer chamber in their study [20]. None of the available systems are efficient to verify large fields. In this study, we used an Octavious phantom, which could measure a dose up to 50cm in length. Two measurements were taken, first in face-in and second in face-out position. Both measurements were composed together to find dose uniformity along the entire length of arcs and the junction of 2 adjacent isocentric arcs. Before verifying the VMAT plan with Octavious phantom, doses were verified with gafchromic films of 5x15cm² along the overlapping region (the study is in progress and not in the scope of the current

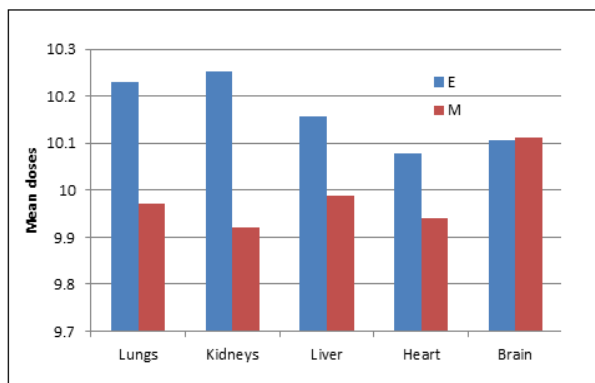


Figure 5. Mean Dose Difference of OARs between two TPSs.

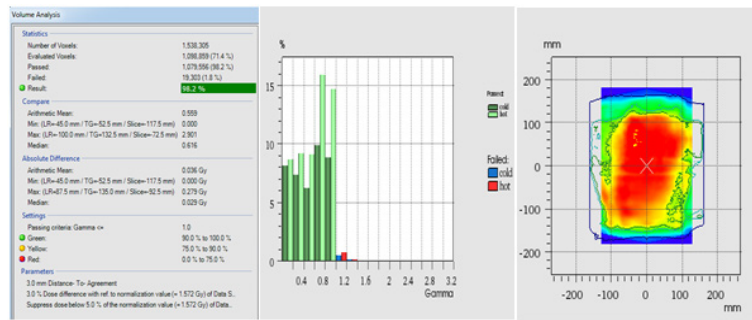


Figure 6. Screenshot Showing Volume Analysis, Gamma, and Dose Distribution Agreement.

Table 5. Brief Comparison of both TPSs:

Parameters compared	Monaco TPS	Eclipse TPS
Optimization and Dose Calculation time	* 4.5 – 6 hrs.	* 21-27 hrs.
Monitor Units	** 6681.2±1210.3	** 2082.3±473.9
Set Up Positioning and Delivery time	1.2 hrs. first day & 35-40 min. rest treatment	1.2 hrs. first day & 40-44 min. rest treatment

*two optimization, ** may be due to algorithm difference

study). Our results are also comparable to those of Zhuang et. al, and Srivastava et.al where it was concluded that gamma analysis (3%, 3mm) with a 10% dose threshold means a good dose comparison between generated and delivered doses [20, 21].

Hence in conclusion we can conclude that both the Eclipse and the Monaco TPSs were capable of a high degree of target dose conformity and critical organ sparing therefore either of the TPS systems can be used for VMAT TBI plan generation. But the planning of VMAT TBI using Monaco is easier as it offers faster optimization on a single target compared to the Eclipse, where sometimes a larger length target is split into 3 to four segments to get a better-quality plan. The MC-based dose calculation accuracy with robust optimization tools in Monaco allowed a much faster generation of VMAT TBI plans. The plan analysis and dosimetric comparison showed the feasibility of VMAT TBI treatment using the Monaco planning software on Versa HD.

The limitations of our study are that it was a dosimetric study, so no clinical information could be derived from our results. The plan analysis and dosimetric comparison showed the feasibility of VMAT TBI treatment using the Monaco planning software on Versa HD. An elaborative planning clinical study is in progress to assess the further scope for improved analysis.

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Approval

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Conflict of Interest

No conflicts of interest.

Ethical Declaration

Yes, approved by institute ethical committee.

Authors Contribution

Reena Sharma: conceptual design, treatment planning, data collection, analysis, manuscript writing and approval.

Dr. Budhi Singh Yadav: conceptual design, patient selection, treatment planning approval, manuscript writing and approval.

Dr. Pankaj Kumar: conceptual design, manuscript writing and approval.

Data Availability

The data that support the finding of this retrospective analysis is available from corresponding author upon reasonable request.

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